INTRODUCTION

Chronic obstructive pulmonary disease (COPD) and asthma are considered distinct diseases. However, they share similar physiologic and clinical features, and they are considered as heterogeneous diseases that often have

Visual and Quantitative Assessments of Regional Xenon-Ventilation Using Dual-Energy CT in Asthma-Chronic Obstructive Pulmonary Disease Overlap Syndrome: A Comparison with Chronic Obstructive Pulmonary Disease

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Objective: To assess the regional ventilation in patients with asthma-chronic obstructive pulmonary disease (COPD) overlap syndrome (ACOS) using xenon-ventilation dual-energy CT (DECT), and to compare it to that in patients with COPD.

Materials and Methods: Twenty-one patients with ACOS and 46 patients with COPD underwent xenon-ventilation DECT. The ventilation abnormalities were visually determined to be 1) peripheral wedge/diffuse defect, 2) diffuse heterogeneous defect, 3) lobar/segmental/subsegmental defect, and 4) no defect on xenon-ventilation maps. Emphysema index (EI), airway wall thickness (Pi10), and mean ventilation values in the whole lung, peripheral lung, and central lung areas were quantified and compared between the two groups using the Student’s t test.

Results: Most patients with ACOS showed the peripheral wedge/diffuse defect (n = 14, 66.7%), whereas patients with COPD commonly showed the diffuse heterogeneous defect and lobar/segmental/subsegmental defect (n = 21, 45.7% and n = 20, 43.5%, respectively). The prevalence of ventilation defect patterns showed significant intergroup differences (p < 0.001). The quantified ventilation values in the peripheral lung areas were significantly lower in patients with ACOS than in patients with COPD (p = 0.045). The quantified Pi10 was significantly higher in patients with ACOS than in patients with COPD (p = 0.041); however, EI was not significantly different between the two groups.

Conclusion: The ventilation abnormalities on the visual and quantitative assessments of xenon-ventilation DECT differed between patients with ACOS and patients with COPD. Xenon-ventilation DECT may demonstrate the different physiologic changes of pulmonary ventilation in patients with ACOS and COPD.

Keywords: Asthma-chronic obstructive pulmonary disease overlap syndrome; Chronic obstructive pulmonary disease; Dual-energy computed tomography; Ventilation; Xenon
overlapping conditions (1-3). Recently, the Global Initiative for Asthma and the Global Initiative for Chronic Obstructive Lung Disease guidelines accepted the concept of asthma-COPD overlap syndrome (ACOS), which is characterized by persistent airflow limitation with several features usually associated with asthma and COPD alone (4). Previous studies have compared the characteristics between patients with ACOS and those with asthma or COPD alone, and have reported that patients with ACOS have more rapid declines in lung function, more frequent exacerbations, higher mortality rates, and greater need for medical resources (1, 5-8). Patients with ACOS may require distinct clinical evaluation and treatment, and their proper management may require an understanding of the pathophysiology of ACOS.

CT is widely used for assessing pulmonary abnormalities in patients with COPD and asthma, and quantitative CT analysis provides objective information about pulmonary parenchymal changes (9-12). Moreover, dual-energy CT (DECT) with xenon-ventilation imaging, which can provide high-resolution anatomic information and pulmonary ventilation status concurrently with single CT scanning, has been used to investigate regional ventilation changes in patients with various obstructive lung diseases including asthma and COPD (13-16). However, no studies have reported the use of DECT or other imaging modalities to assess the parenchymal ventilation changes in patients with ACOS. Therefore, we aimed to assess the regional ventilation status in patients with ACOS by using xenon-ventilation DECT and to compare it to that of patients with COPD.

MATERIALS AND METHODS

Patients
This prospective study was approved by our Institutional Review Board. Written informed consent was obtained after the explanation of the study and the disclosure of the patients’ clinical information. Between May 2012 and December 2016, we recruited 21 patients with ACOS and 46 patients with COPD from our pulmonology clinic. The diagnoses of ACOS and COPD were made by a pulmonologist according to the joint statement released by the Global Initiative for Asthma and the Global Initiative for Chronic Obstructive Lung Disease (4). Among these patients, 27 patients with COPD were included in the previous study (15). All patients underwent xenon-ventilation DECT, pulmonary function test (PFT) with a spirometer, diffusion capacity measurement, and the 6-minute walk distance test (6MWT) on the same day.

Xenon-Ventilation DECT and Postprocessing
Patients inhaled 30% stable xenon gas using a face mask designed for positive pressure ventilation treatments (King Systems Corporation, Noblesville, IN, USA) and a xenon gas inhalation system (Zetron V, Anzai Medical, Tokyo, Japan). We monitored xenon concentration in the inhaled and exhaled gases throughout the study. After the xenon concentration in the exhaled gas reached 25%, a full-thoracic CT was performed using the SOMATOM Flash CT (Siemens Healthineers, Forchheim, Germany) (55/130 eff. mA at sn140/80 kV, 64 x 0.6 mm collimation, 0.55 pitch, and 0.2-second rotation time) (15). A detailed description about CT protocol can be found in the Supplementary Materials.

In postprocessing, virtual non-contrast (VNC) images and xenon-ventilation maps were obtained from the 80- and Sn140-kV images using the modified “liver VNC” and “xenon” applications of Syngo Dual Energy (Siemens Healthineers). Image data were reconstructed with a 1.5-mm section thickness using kernel D30 at 1.5-mm increments.

Visual Analysis of Xenon-Ventilation Patterns
Xenon-ventilation in the lung parenchyma was displayed on the color-coded xenon-ventilation maps by using the xenon-attenuation value. The two axial image sets (VNC image and xenon-ventilation map) were simultaneously displayed using in-house software. The presence of ventilation defects was judged based on the normal lung findings on the xenon-ventilation maps from a previous study (13). Areas enhanced by xenon were displayed as orange, yellow, and green, and were interpreted as showing normal ventilation. Areas with poor or no enhancement by xenon were displayed as blue or purple on our xenon-ventilation maps (Fig. 1). Blue-to-purple-colored areas, which were sharply demarcated from normal yellow-to-green areas, indicated ventilation defects. Two chest radiologists (with 11 and 9 years of experience in thoracic radiology, respectively), blinded to the diagnosis of cases, determined the xenon-ventilation abnormality patterns in consensus to represent 1) peripheral wedge/diffuse defects (ventilation defects not extending to the hilum or central lung areas), 2) diffuse heterogeneous defects (ventilation defects and normal ventilation areas intermixed throughout the lungs), 3) lobar/segmental/subsegmental defects (ventilation defects extending to the hilum or central lung areas).
defects extending to the hilum or central lung area with lobar, segmental, or subsegmental distribution), and 4) no defects (Fig. 1). We categorized these patterns according to the descriptions in the previous studies (13-15, 17, 18). If one patient had any two or three intermixed ventilation patterns, the most predominant pattern was used to describe the abnormality. Areas of parenchymal abnormality on VNC images, possibly showing ventilation abnormalities such as atelectasis or sequelae, were excluded during the visual assessment of ventilation defects. The highest and lowest ventilation values in the regions at the thoracic wall (dorsal part) and around the heart were thought to have been caused by the inherent artifacts from the current dual-source DECT acquisition, including offset of acquisition between two different X-ray tubes and beam-hardening artifact. We excluded such regions from the visual analysis.

**Quantitative Analysis of Ventilation and Quantitative CT Densitometry**

Ventilation values on xenon-ventilation DECT were quantified using in-house software. After the automatic extraction of the whole lung, the ventilation values, i.e., the mean Hounsfield unit (HU) of the xenon map in the lung parenchyma, of the whole lung area were quantified. The whole lung was divided into the peripheral and central lungs using theoretical lung surface lines drawn at 20-mm depths from the lung surface (19). Thereafter, the ventilation values in the peripheral and central lung areas were quantified. The emphysema index (EI; the percentage of the area below -950 HU in the lung parenchyma) (20-22) and airway measurement were determined using commercial software (Aview, Coreline Soft, Seoul, Korea) on VNC images. For airway measurement, Pi10, which is the square root of the wall area of the theoretical airway with a 10-mm internal perimeter (23), was obtained using the integral-based half-band algorithm (24). We obtained the Pi10 value by creating regression plots of the square root of the wall area against the corresponding internal perimeter of the 5th–8th branches of the airways in all segments of both lungs (25).

**Statistical Analysis**

Baseline characteristics, PFT and 6MWT results, and quantified CT parameters were compared between the ACOS and COPD groups by using Student’s t test. The prevalence of ventilation abnormality patterns was compared between the groups by using the χ² test. Pearson’s correlation analysis was used to compare the quantified CT values and PFT results. All statistical analyses were performed...
using SPSS version 21.0 (IBM Corp., Armonk, NY, USA). The quantified variables are expressed as means ± standard deviation. \( P < 0.05 \) indicated statistical significance.

**RESULTS**

**Patients’ Characteristics**

The patients’ clinical characteristics are summarized in Table 1. No significant intergroup differences were observed in age, body mass index, smoking history, and PFT and 6MWT results, except for the carbon monoxide diffusing capacity corrected for hemoglobin concentration (DL\(_{CO}\)), which was significantly higher in the ACOS group than in the COPD group.

**Visual Analysis of Xenon-Ventilation Patterns**

On visual analysis, all patients showed morphologic abnormalities such as emphysema, bronchial wall thickening, or parenchymal air trapping on VNC images. The CT findings on VNC images were visually indistinguishable between the ACOS and COPD groups.

All patients in the ACOS and COPD groups showed diffuse or regional ventilation abnormalities on the xenon-ventilation maps. Ventilation abnormalities in patients with ACOS most often appeared as peripheral wedge/diffuse defects (14/21, 66.7%), which were seen mostly in the periphery of the middle-to-lower lung areas and had a wedge-shaped or diffuse configuration (Figs. 1, 2). In this pattern, the ventilation defects were confined to the peripheral half or one-third of the pleural surface of the lung parenchyma. The boundaries of most ventilation defects were well demarcated from the surrounding normally ventilated lung. The areas without ventilation defects mostly showed homogeneous xenon enhancement in patients with ACOS. In patients with COPD, peripheral wedge/diffuse defects were only seen in 5 of 46 (10.9%), and diffuse heterogeneous defects (21/46, 45.7%) were the most common, followed by lobar/segmental/subsegmental defects (20/46, 43.5%). In the diffuse heterogeneous defect pattern, ventilation defects were seen throughout the lung, with a mixture of small areas with normal and poor ventilation. Lobar/segmental/subsegmental defects in patients with COPD mostly involved one segment and extended into the central half of the lung. In some patients with COPD, both diffuse heterogeneous defects and lobar/segmental/subsegmental defects were seen concurrently. The prevalence of the three patterns showed significant intergroup differences (\( p < 0.001 \)) (Table 2).

**Quantitative Analysis of Xenon-Ventilation and Quantitative CT Densitometry**

The quantified ventilation value of the peripheral lung area was significantly lower in the ACOS group than in the COPD group (\( p = 0.045 \)); however, the values of the whole and central lung areas showed no significant intergroup differences (Table 3). The mean EI values of the whole lung

### Table 1. Demographic Information and Pulmonary Function Test Results in ACOS and COPD Groups

<table>
<thead>
<tr>
<th>Variables</th>
<th>ACOS (n = 21)</th>
<th>COPD (n = 46)</th>
<th>( P^* )</th>
</tr>
</thead>
<tbody>
<tr>
<td>Age (years)</td>
<td>66.1 ± 7.6</td>
<td>67.4 ± 7.2</td>
<td>0.504</td>
</tr>
<tr>
<td>Sex (n) M:F = 20:1</td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Body mass index (kg/m(^2))</td>
<td>24.4 ± 2.9</td>
<td>23.8 ± 3.0</td>
<td>0.482</td>
</tr>
<tr>
<td>Smoking history (pack-years)</td>
<td>43.1 ± 25.2</td>
<td>41.5 ± 13.4</td>
<td>0.729</td>
</tr>
<tr>
<td>FEV(_1) (%pred)</td>
<td>54.8 ± 11.0</td>
<td>55.1 ± 14.1</td>
<td>0.932</td>
</tr>
<tr>
<td>FVC (%pred)</td>
<td>85.5 ± 10.8</td>
<td>84.2 ± 12.7</td>
<td>0.700</td>
</tr>
<tr>
<td>FEV(_1)/FVC (%)</td>
<td>45.8 ± 8.8</td>
<td>46.7 ± 11.9</td>
<td>0.750</td>
</tr>
<tr>
<td>DL(_{CO}) (corrected %pred)</td>
<td>74.0 ± 12.6</td>
<td>64.2 ± 19.7</td>
<td>0.042( ^\dagger )</td>
</tr>
<tr>
<td>TLC (%pred)</td>
<td>101.4 ± 11.3</td>
<td>95.9 ± 13.8</td>
<td>0.119</td>
</tr>
<tr>
<td>VC (%pred)</td>
<td>98.2 ± 12.9</td>
<td>96.4 ± 14.4</td>
<td>0.627</td>
</tr>
<tr>
<td>FRC (%pred)</td>
<td>119.3 ± 22.5</td>
<td>118.6 ± 26.6</td>
<td>0.915</td>
</tr>
<tr>
<td>RV (%pred)</td>
<td>106.7 ± 29.9</td>
<td>96.4 ± 32.7</td>
<td>0.226</td>
</tr>
<tr>
<td>6MWT (m)</td>
<td>480.6 ± 66.4</td>
<td>465.9 ± 79.8</td>
<td>0.465</td>
</tr>
</tbody>
</table>

Values are expressed as means ± standard deviation. 6MWT data are available for 45 patients. *Comparison between ACOS and COPD groups is performed using Student’s t test. †Value is statistically significant (\( p < 0.05 \)). ACOS = asthma-COPD overlap syndrome, COPD = chronic obstructive pulmonary disease, DL\(_{CO}\) = carbon monoxide diffusing capacity corrected for hemoglobin concentration, FEV\(_1\) = forced expiratory volume in 1 second, FRC = functional residual capacity, FVC = forced vital capacity, m = meter, NA = not applicable, RV = residual volume, TLC = total lung capacity, VC = vital capacity, 6MWT = 6-minute walk distance test, %pred = percentage predicted value
were 7.7 ± 6.6% in the ACOS group and 12.0 ± 12.4% in the COPD group. The EI showed no significant intergroup differences (p = 0.070); however, the ACOS group showed a tendency towards a lower EI than did the COPD group. The average Pi10 measurements in the ACOS and COPD groups were 5.04 ± 0.55 and 4.66 ± 0.72, respectively; the segmental airways were thicker in the ACOS group than in the COPD group (p = 0.041).

**Correlation between Quantified CT Parameters and PFT Results**

The ventilation value of the central lung area showed a significant positive correlation with the forced expiratory volume in 1 second (FEV1) in patients with ACOS (r = 0.499, p = 0.025). The value of the whole lung area also showed a tendency towards a positive correlation with FEV1; however, the EI showed no significant differences between groups.

**Table 2. Visual Analysis of Ventilation Defect Patterns in Patients with ACOS and COPD**

<table>
<thead>
<tr>
<th>Disease</th>
<th>Pattern (1)</th>
<th>Pattern (2)</th>
<th>Pattern (3)</th>
<th>p*</th>
</tr>
</thead>
<tbody>
<tr>
<td>ACOS (n = 21)</td>
<td>14 (66.7)</td>
<td>2 (9.5)</td>
<td>5 (23.8)</td>
<td>&lt; 0.001†</td>
</tr>
<tr>
<td>COPD (n = 46)</td>
<td>5 (10.9)</td>
<td>21 (45.7)</td>
<td>20 (43.5)</td>
<td></td>
</tr>
</tbody>
</table>

Data are numbers of patients with percentages in parentheses. *Comparison between ACOS and COPD groups is performed using χ² test. †Value is statistically significant (p < 0.05). Pattern (1), peripheral wedge/diffuse defect; Pattern (2), diffuse heterogeneous defect; Pattern (3), lobar/segmental/subsegmental defect.

**Fig. 2. Peripheral wedge/diffuse defect pattern of xenon-ventilation in 54-year-old man with ACOS (emphysema index = 5.73, square root of wall area of airway with 10-mm internal perimeter = 5.42).**

A, B. Axial and coronal weighted average images of dual-energy CT show diffuse bronchial wall thickening with minimal centrilobular emphysema. C, D. Axial and coronal xenon-ventilation maps show multifocal wedge-shaped or patchy areas showing blue-to-purple color in peripheral lung areas, indicating ventilation defects (arrowheads). We considered linear or ovoid or patchy-shaped black-, purple-, blue-, or red-colored areas around vertebral body, heart, and dorsal part of lung on xenon map as artifacts. We excluded these areas from visual analysis. ACOS = asthma-chronic obstructive pulmonary disease overlap syndrome.
it was not statistically significant ($r = 0.286, p = 0.222$) (Fig. 3A, B, Supplementary Table 1). The value of the peripheral lung area was not significantly correlated with FEV1. The EI showed negative correlations with FEV1/forced vital capacity (FVC) and DLCO ($r = -0.510, p = 0.018$ and $r = -0.445, p = 0.043$, respectively) in patients with ACOS. The EI also showed a tendency towards a negative correlation with FEV1; however, it was not statistically significant ($r = -0.310, p = 0.171$) in the ACOS group. In patients with COPD, the EI showed significant negative correlations with FEV1, FEV1/FVC, DLCO, and 6MWT results, and the ventilation values of the whole, central, and peripheral lung areas showed significant positive correlations with most of the PFT results (Fig. 3C, D, Supplementary Table 2).

DISCUSSION

Our study showed that the xenon-ventilation DECT may demonstrate different ventilation abnormalities predominantly seen in patients with ACOS or COPD. Fourteen of 21 patients with ACOS showed the wedge/diffuse ventilation defects in the periphery of the mid-to-lower lungs. However, most patients with COPD showed diffuse heterogeneous defects throughout the lung or lobar/segmental/subsegmental defects. The quantified xenon-ventilation value of the peripheral lung areas was also significantly lower in patients with ACOS than in patients with COPD. The values of the whole and central lung areas showed a tendency towards a positive correlation with FEV1, with the central lung values showing statistical significance.

Parenchymal ventilation abnormalities in the obstructive lung diseases have been investigated using various imaging modalities, such as magnetic resonance imaging (MRI), single-photon emission computed tomography, and DECT (13, 14, 26-32). Although static anatomic imaging is dominant in clinical practice, the functional imaging evaluating parenchymal ventilation may enhance our understanding of physiologic changes or structural-functional relationships in the obstructive lung diseases, as well as physiologic changes after treatments (33). DECT has advantages in providing both high-resolution anatomic information and functional information with single CT scanning. To our knowledge, the ventilation abnormalities in patients with ACOS have not been documented at a morphologic level, and we investigated the ventilation abnormalities in patients with ACOS by using xenon-ventilation DECT and compared them to those in patients with COPD. Although patients with ACOS and COPD could not be discriminated using VNC images, patients with ACOS mostly showed the peripheral wedge/diffuse ventilation defects on xenon-ventilation maps, unlike patients with COPD.

The predominant ventilation defect patterns in each group differed in our study, even though both groups shared some ventilation defect patterns on xenon-ventilation DECT. The precise pathophysiology of ventilation defects on various ventilation imaging remains unclear, and the authors of the previous studies explained and estimated the causes of ventilation defect patterns according to the pathophysiologic characteristics of each disease. The peripheral wedge ventilation defect is frequently seen on various ventilation images performed in asthmatics (14, 34). Since asthma is characterized by mucus hypersecretion, airway hyperreactivity, and airway edema, it seems likely that the cause of the peripheral wedge ventilation defects in asthmatics is small airway obstruction from some combination of these factors (34, 35). In these subjects, the ventilation defects also reversed following bronchodilator inhalation, and this reversal is likely due to dilation of the small airways, allowing air to pass through previously constricted airways (16, 35). The heterogeneous or patchy or lobar/segmental/subsegmental defects have been reported in the COPD group (13, 15), and these patterns may be seen in one patient at the same

Table 3. Quantitative Analysis of Xenon-Ventilation and Quantitative CT Densitometry in Patients with ACOS and COPD

<table>
<thead>
<tr>
<th>Variables</th>
<th>ACOS</th>
<th>COPD</th>
<th>P*</th>
</tr>
</thead>
<tbody>
<tr>
<td>Emphysema index (%)</td>
<td>7.7 ± 6.6</td>
<td>12.0 ± 12.4</td>
<td>0.070</td>
</tr>
<tr>
<td>Airway measurement (Pi10) (mm)</td>
<td>5.0 ± 0.6</td>
<td>4.7 ± 0.7</td>
<td>0.041†</td>
</tr>
<tr>
<td>Ventilation_whole lung (HU)</td>
<td>22.2 ± 2.2</td>
<td>23.3 ± 3.7</td>
<td>0.130</td>
</tr>
<tr>
<td>Ventilation_peripheral lung (HU)</td>
<td>21.3 ± 2.3</td>
<td>22.8 ± 3.7</td>
<td>0.045†</td>
</tr>
<tr>
<td>Ventilation_central lung (HU)</td>
<td>24.1 ± 2.4</td>
<td>24.4 ± 4.1</td>
<td>0.710</td>
</tr>
</tbody>
</table>

Values are expressed as means ± standard deviation. *Comparison between ACOS and COPD groups is performed using Student’s t test. †Value is statistically significant ($p < 0.05$). HU = Hounsfield unit, Pi10 = square root of wall area of airway with 10-mm internal perimeter.
time. COPD is characterized by a loss of parenchymal recoil, and thus hyperinflation, peripheral airway obstruction, airway inflammation resulting in obstruction of both large and small airways, and various combinations of these factors are thought to be responsible for the ventilation defects in COPD. Since the predominant ventilation defect pattern in the ACOS group was like that in asthmatics, the similar etiology may be associated with the characteristic ventilation defect pattern in the ACOS group. Although the airway disease in ACOS may have the characteristics of both COPD and asthma, the characteristics of small airway disease that may result in ventilation defects in ACOS may be similar to those of asthma.

Our study showed that thicker segmental airways (higher Pi10) are associated with the patients with ACOS, even though our patient groups were matched for their demographic characteristics and baseline PFT characteristics. The emphysema severity showed no intergroup difference; however, the ACOS group showed a tendency towards a lower EI than did the COPD group. These findings are similar
to the results of the previous studies (2, 36, 37). Currently, we cannot precisely explain why the thicker segmental airways are seen in the ACOS group compared with the COPD group. However, these results may suggest that ACOS is an airway-dominant disease rather than an emphysema-dominant disease as compared to COPD. Using CT, COPD is characterized as a heterogeneous group that can be divided into emphysema-dominant, airway disease-dominant, or mixed types. Patients with ACOS showed more significant reversibility in the CT-quantified airway wall thickening and air trapping in response to bronchodilator than did patients with COPD in the previous studies (36, 37). These results also suggest that ACOS is a more airway-dominant disease than is COPD. In addition, as we discussed above, the characteristics of airway disease in ACOS may be more like those of asthma than those of COPD. The wall thickness and wall area on CT were greater in asthmatics than in COPD patients in the previous study (38). The relationship between structural and functional airway changes of ACOS patients compared with COPD patients and asthmatics requires further study.

The introduction of $^{129}$Xe- or $^3$He-ventilation MRI and xenon-ventilation DECT has enabled the investigation of ventilation abnormalities in asthma and COPD (13-15, 27, 28, 35, 39, 40). These abnormalities are readily demonstrated as decreased signal intensity on $^3$He-MRI or $^{129}$Xe-MRI, and the number and size or percentage of these abnormalities correlate with disease severity or FEV$_1$ (27, 28, 35, 40). Xenon-ventilation DECT demonstrates the decreased xenon-enhancement, which can be quantified as the ventilation value. These quantified ventilation values significantly correlated with the clinical parameters of patients with COPD (15, 21); however, they were not significantly correlated with the FEV$_1$ in asthmatics (41). We quantitatively assessed xenon-ventilation in various lung areas, and it tended to correlate with the PFT results more in patients with COPD than in those with ACOS, despite similar correlation tendencies between the two groups. However, our study was limited by its small number of patients with ACOS; hence, further studies with larger numbers of patients with ACOS are warranted.

Our study has several limitations. First, the ACOS group was relatively small because this was a single-center study. Second, some $p$ values (Pi10 and ventilation value in the peripheral lung) of the comparison of CT quantitative values between the ACOS and COPD groups were marginal. However, also in the previous study, ACOS patients had higher wall area percentage (37). Further studies with larger sample sizes are needed for validating this issue. Third, the diagnosis of ACOS was partly based on a retrospective assessment of asthma-related symptoms. Although all our patients with ACOS in this study were diagnosed by an expert pulmonologist, distinguishing ACOS from COPD might be difficult in some patients. Fourth, the consensus visual analysis of xenon-ventilation patterns without validation of the reproducibility or interobserver agreement could be a limitation, although radiologists who experienced in xenon-ventilation image analysis and research performed the visual analyses. Fifth, we used the multiple breath-in method, which might possibly obscure the ventilation defects that can be seen on $^3$He-MRI using the single breath-in method. However, xenon attenuation with the single breath-in method on DECT was too low; therefore, the multiple breath-in method was required to acquire images with sufficient attenuation for the visual and quantitative analyses. Sixth, we used VNC images to quantify the EI and airway wall thickening. The HU on VNC images may not be identical to that of actual non-contrast CT images. However, a previous study showed a correlation between the quantified parameters of VNC images and PFT results (42). In conclusion, our study demonstrated the potential of xenon-ventilation DECT, as it shows the different ventilation abnormalities visually and quantitatively in patients with ACOS compared to patients with COPD. Xenon-ventilation DECT can demonstrate different physiologic changes in pulmonary ventilation in patients with ACOS and COPD.

**Supplementary Materials**

The Data Supplement is available with this article at https://doi.org/10.3348/kjr.2019.0936.

**Conflicts of Interest**
The authors have no potential conflicts of interest to disclose.

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